

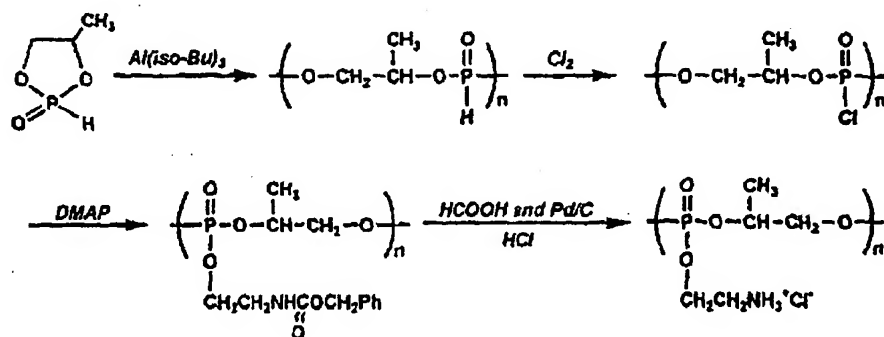
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(54) Title: BIODEGRADABLE POLYPHOSPHATES FOR CONTROLLED RELEASE OF BIOACTIVE SUBSTANCES



(57) Abstract: The present invention is directed to a biodegradable system for the controlled release of bioactive substances. This system comprises novel biodegradable and biocompatible polyphosphoesters that carry positive charges. Process for making these polyphosphoesters, compositions containing these polyphosphoesters and biologically active substances, articles and methods for delivery of drugs and genes using this system are described. A controlled gene delivery system based on these polyphosphoesters is prepared by complex coacervation of nucleic acid (DNA or RNA) with polymers. The release rates can be manipulated by adjusting the charge ratios of polyphosphoesters to nucleic acids. This gene delivery system yields a higher gene expression in muscle when injected intramuscularly.

## 5     BIODEGRADABLE POLYPHOSPHATES FOR CONTROLLED RELEASE OF BIOACTIVE SUBSTANCES

          This application claims the benefit of U.S. Provisional Application Serial No.  
60/290,888 filed May 14, 2001, the teachings of which are incorporated herein by  
10   reference.

### BACKGROUND OF THE INVENTION

#### 1.     Field of the Invention

          The present invention generally relates to biodegradable polymer compositions, in  
15   particular those containing both phosphoester linkages in the polymer backbone and  
chargeable groups linked to the backbone through a phosphoester bond. These  
biodegradable polymers of the invention are designed for the controlled release of drugs  
and genes, particularly as carriers for gene therapy and for the delivery of protein drugs.  
The invention also has wide applicability in tissue engineering applications, where the  
20   sustained delivery of growth factors is achieved through gene transfer.

#### 2.     Background

          Polymeric controlled drug delivery has significantly improved the success of  
many drug therapies (*Langer, 1990, New methods of drug delivery, Science 249: 1527-*  
25   *33; Poznansky, et al., 1984, Biological approaches to the controlled delivery of drugs: a*  
*critical review, Pharmacol. Rev. 36: 277-336*). In such a delivery system,  
pharmacokinetics and biodistribution of the drug depend upon the physiochemical  
properties and/or degradation properties of the polymer carriers. In general, polymeric  
carriers offer advantages over other delivery systems: polymeric systems potentially have  
30   more controllable release kinetics, better stability in storage, and have better  
biocompatibility. A biodegradable drug-carrier could offer features difficult to attain  
from non-biodegradable systems. Other than obviating the need to remove the drug-

depleted devices, a biodegradable system is also applicable to a wider range of drugs. More and more new polymer carriers have been proposed for controlled drug delivery, although poly(lactide-co-glycolide) copolymers still dominate the field. There is clearly justification to continue to develop new biodegradable drug-carriers, because of the  
5 increasing need in the emerging new applications. The widening scope of applications requires polymeric carriers to assume different configurations and serve additional functions other than just passive delivery. For instance, applying the controlled release device as more than just a monolithic matrix, for example, as a coating material for a drug-eluting stent, may obligate the polymer to have elastomeric properties. In the new  
10 and exciting field of tissue engineering where local and sustained delivery of growth factors and/or genes encoding these growth factors may influence the course of tissue development, the drug-carrier may also need to perform a double-duty to provide structural support or scaffolding functions. To achieve active targeting, it would involve conjugation of ligands to the polymeric carriers, which requires the polymeric carrier to  
15 contain functional groups for derivatization. In the field of gene delivery, polymeric gene carriers need to be of polycationic nature and should have the structural flexibility to include targeting feature and parameters affecting the intracellular trafficking of the genes (*Han, et al., 2000, Development of biomaterials for gene therapy, Molecular Therapy 2: 302-317; Varga, et al., 2000, Receptor-mediated targeting of gene delivery vectors: insights from molecular mechanisms for improved vehicle design. Biotechnol. Bioeng. 70: 593-605*).  
20 With such a broad utility for these biodegradable drug-carriers, no one single material can be expected to satisfy all requirements of different applications.

Gene therapy has been progressively developed with the hope that it will be an  
25 integral part of medical modalities in the future. Gene delivery system is one of the key components in gene medicine, which directs the gene expression plasmids to the specific locations within the body. The control of gene expression is achieved by influencing the distribution and stability of plasmids *in vivo* and the access of the plasmids to the target cells, and affecting the intracellular trafficking steps of the plasmids  
30 (*Mahato, et al., 1999, Pharmaceutical perspectives of nonviral gene therapy, Adv. Genet. 41: 95-156*). Recently, there is an increasing interest in developing systems for sustained

release of DNA. Such a system could be used to achieve localized and enhanced gene expression in skeletal muscle. It would find wide applications in treating muscle and nerve disorders, providing systemic circulation of secretory proteins, and as a genetic vaccine carrier. Encapsulation of DNA in PLGA nanoparticles (Cohen, et al., 2000, Sustained delivery and expression of DNA encapsulated in polymeric nanoparticles. Gene Therapy 7: 1896-1905) and absorption of plasmid to the surface of cationic PLGA microparticles (Singh, et al., 2000, Characterization of cationic microparticles with adsorbed plasmid DNA. Proceed. Int'l. Symp. Control. Rel. Bioact. Mater., 27: 6405-6406) have been reported recently to achieve sustained release of plasmid DNA. Sustained release of DNA was observed for 2 to 4 weeks in these systems. The cationic microparticles induced about four-fold higher gene expression level in muscle at day 14, and induced higher Th1 and Th2 responses in mice (Singh, et al., 2000, Cationic microparticles: A potent delivery system for DNA vaccines. Proc. Natl. Acad. Sci. USA 97(2): 811-816). However, both systems are limited by the low DNA loading levels (<1%) and the little room for optimization of DNA release kinetics. Other systems currently under investigations are non-biodegradable polymeric systems, e.g. poly(ethylene-co-vinyl acetate) (Luo, et al., 1999, Controlled DNA delivery systems. Pharm. Res. 16(8): 1300-1308) and Poloxamers (Lemieux, et al., 2000, A combination of poloxamers increases gene expression of plasmid DNA in skeletal muscle. Gene Therapy 7: 986-991). The present patent features a novel gene delivery system that based on the biodegradation of polymeric carriers to achieve a sustained release of plasmid DNA in a controlled manner.

#### SUMMARY OF THE INVENTION

25 The invention provides positively chargeable biodegradable polymers that comprises at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage.

30 The invention further provides positively chargeable biodegradable polymer compositions comprising:

- (a) at least one biologically active substance; and
- (b) A positively chargeable biodegradable polymer comprising at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage.

The invention additionally provides a method of preparing a positively chargeable biodegradable polymers. The method comprising the steps of:

- polymerizing at least one monomer to form a polymer with at least one phosphoester linkage in the polymer backbone;
- reacting the polymer with an alcohol having a positively chargeable group or a substituent that can be functionalized to a positively chargeable group under conditions conducive to the formation of a positively chargeable biodegradable polymer comprising at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage.

The invention provides a method of preparing a positively chargeable biodegradable polymer composition. The method comprises the steps of:

- providing a positively chargeable biodegradable polymer comprising at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage.
- contacting the positively chargeable biodegradable polymer with a biologically active substance under conditions conducive to the formation of a complex comprising the positively chargeable biodegradable polymer and the biologically active substance.

The invention also provides for the controlled release of a biologically active substance in-vivo or in-vitro. The method comprises the steps of:

- providing a positively chargeable biodegradable polymer composition comprising:
  - (a) at least one biologically active substance; and

(b) A positively chargeable biodegradable polymer comprising at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage;

- 5           contacting the composition in vivo or in vitro with a biological fluid, cell or tissue under conditions conducive to the delivery of at least a portion of the biologically active substance to the biological fluid, cell or tissue. .

The invention further provides methods for gene transfection using the controlled  
10   release methods and the positively chargeable biodegradable polymer composition comprising a DNA sequence, a gene or a gene fragment, to deliver a DNA sequence, a gene or a gene fragment to a specified tissue target in a patient. Gene transfection methods of the invention are suitable for use in treatment of any disease or disorder which is currently treatable by gene therapy or is contemplated as a disease or disorder suitable  
15   for treatment by gene therapy in the for future. Gene transfection methods of the invention comprise the steps of

          providing a positively chargeable biodegradable polymer composition comprising:

- (a)     at least one biologically active substance; and  
          (b)     A positively chargeable biodegradable polymer comprising at least one  
20   phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage;

          contacting the composition with a biological fluid, cell or tissue under conditions conducive to the delivery of at least a portion of the DNA sequence, gene or gene  
25   fragment to the biological fluid, cell or tissue.

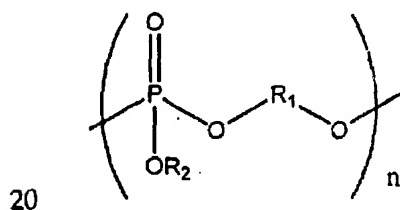
#### BRIEF DESCRIPTION OF THE DRAWINGS:

- Figure 1. Synthesis scheme of PPE-EA;  
Figure 2. Gel permeation chromatograph of PPE-EA;  
30   Figure 3. Cytotoxicity of PPE-EA in COS-7 Cells as compared with PEI and PLL;  
Figure 4. Gel electrophoretic analysis of the complexation of PPE-EA with DNA;

- Figure 5. *In vitro* release profiles of plasmid DNA from PPE-EA-DNA coacervates prepared at different charge ratios;
- Figure 6. *In vitro* transfection efficiency of PPE-EA-DNA coacervates in HEK 293 cells;
- 5 Figure 7. Beta-galactosidase level in mouse muscle following intramuscular injection of PPE-EA-DNA coacervates at a dose of 2 µg DNA/muscle;
- Figure 8. Tissue response at day 7 following intramuscular injection of PPE-EA and PEL. (a) Saline injection (40 µl), showed normal tissue; (b) & (c): PPE-EA injection (13.1 µg, 60 nmole amino group), showed focal inflammation; (d) &
- 10 (e): PEI (Mw 25 KDa, 2.5 µg, 60 nmole charged groups), showed severe inflammation and muscle necrosis; and
- Figure 9. IFN-α2b concentration in serum of mice following intramuscular injection of naked DNA (n = 5~7) or complexes at N/P ratio of 0.5 (n = 5~7). Each mouse received a dose equivalent to 50 µg of plasmid DNA. Naïve mice served as a
- 15 control (n=4).

#### DETAILED DESCRIPTION OF THE INVENTION

The biodegradable polyphosphoesters of the invention comprise the recurring monomeric units shown in the Formula I:



FORMULA I

wherein:

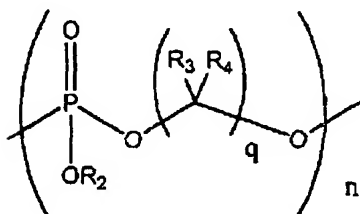
- R<sub>1</sub> is a divalent organic moiety that is aliphatic, aromatic or heterocyclic;
- 25 R<sub>2</sub> is alkyl, aryl, heteroaryl, heteroalicyclic, cycloalkyl, aralkyl, or cycloalkylalkyl;
- and

each occurrence of  $R_2$  is substituted with one or more positively chargeable functional groups (e.g. primary amino group, secondary amino group, tertiary amino group and quaternary amino group, etc.); and

$n$  is 5 to 2000.

5

Particularly preferred polymers according to formula I include polymers of formula II:



FORMULA II

10 wherein:

$R_2$  is as defined in Formula I;

$R_3$  and  $R_4$  are independently selected at each occurrence of  $R_3$  and  $R_4$  from the group consisting of hydrogen, alkyl, cycloalkyl, alkoxy, aryl, heteroaryl, heteroalicyclic, aralkyl, a steroid derivative; and

15  $q$  is an integer from about 1 to about 5.

Preferred positively chargeable biodegradable polymers of the invention are capable of forming a complex with negatively charged or neutral biologically active substances. Preferred biologically active substances include DNA, RNA, proteins, small molecule therapeutics, and the like.

Other preferred positively chargeable biodegradable polymers of the invention include polymers capable of complexing 20-60% by weight of a negatively charged or neutral biologically active substance such as DNA, RNA, proteins, small molecule therapeutics, and the like.



Furthermore, preferred positively chargeable biodegradable polymers of the invention include polymers having between about 5 and about 2,000 phosphate groups, more preferably between about 10 and about 1500 phosphate groups, and particularly preferred are polymers having between about 20 and 1000 phosphate groups. Also  
5 preferred are polymers having a molecular weight of between about 1000 and 500,000, more preferably having a molecular weight of between about 2000 and 200,000, particularly preferable are polymers having a molecular weight of between about 2000 and 100,000.

10 In additional preferred embodiments, positively chargeable biodegradable polymers of the invention further comprise one or more groups that facilitate intracellular or extracellular delivery of a negatively charged or neutral biologically active substance. Preferred groups for facilitating intracellular delivery of a biologically active substance include a lysosomalytic agent, an amphiphilic peptide, a steroid derivative, and the like.

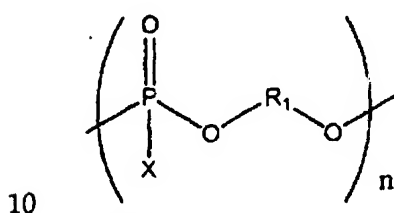
15 In preferred embodiments, the biodegradable polyphosphoester polymers of the invention, including polymers according to Formula I or Formula II, are biocompatible before and upon degradation.

20 In another embodiment, the invention features a coacervate system useful for the delivery of bioactive macromolecules comprising the biodegradable polymer of Formula I.

25 In a further embodiment, the invention contemplates a process of making polymeric coacervates for delivery of bioactive macromolecules.

In yet another embodiment, the invention comprises articles comprising one or several different polymers with structures shown in Formula I and bioactive substances, e.g. nucleic acids and other negatively charged macromolecules for sustained release of these  
30 bioactive substances in-vivo and in-vitro. Additionally, the bioactive substances can be released in a controlled, sustained manner either an intracellular and extracellular manner.

In a still further embodiment, the invention contemplates a process for preparing biodegradable polyphosphoesters, which comprises a step of reacting a polymer shown in Formula III, wherein X is a halogen and R<sup>1</sup> is as defined in Formula I, with an alcohol  
 5 having a general structure as R<sup>2</sup>OH, wherein R<sub>2</sub> is alkyl, aryl, heteroaryl, heteroalicyclic, cycloalkyl, aralkyl or cycloalkylalkyl wherein each occurrence of R<sub>2</sub> is substituted with one or more positively chargeable functional groups (e.g. primary amino group, secondary amino group, tertiary amino group and quaternary amino group, etc.).



FORMULA III

In specific embodiments, one or more charged groups present in R<sub>2</sub> are capable of reacting with a P-halogen bond. Preferably, reactive charged groups are protected using  
 15 standard organic chemistry protecting group techniques. The protected alcohol, R<sub>2</sub>OH, is then reacted with the polymer of Formula III. In particularly preferred embodiments, reactive charged groups include primary or secondary amine groups.

The biodegradable polymeric system described in the present invention achieves  
 20 sustained and localized delivery of one or more therapeutic agents to a designated biological tissue or site in a patient. In particular, the polymeric system of the invention achieves sustained and localized delivery of one or more genes in skeletal muscles or intradermally and achieve a higher gene transfer efficiencies than other plasmid delivery systems currently under investigation.

25

The polyphosphate carriers of the present invention typically offer the following advantages over other biodegradable carriers described in the literature and patents:

The polyphosphate carriers of the present invention are more efficient at binding to nucleic acids and proteins. In general, polymers provided herein have higher molecular weight than most other biodegradable carriers and a relatively high charge density, which leads to an increased binding capacity to plasmid DNA. Increased DNA binding capacity results in increased nucleic acid loading levels for the polyphosphate carriers provided herein. Compared to the PLGA microparticle systems reported in the literatures, the coacervate system provided by the present invention is capable of much higher loading levels of nucleic acids (in a range of 20 to 60%, as compared with less than 1% for the microparticle systems reported in the literatures). This is particularly beneficial when a higher dose of administration is needed.

The structures of the polyphosphate carriers of the present invention can be modified to have variable charge groups with different pKb, different charge density, molecular weight, hydrophilicity/hydrophobicity balance to optimize the *degradation rate of the polymers, nucleic acid release rates from the systems and transfection activity of the polymers*. Sustained release of plasmid DNA is achieved either *in an extracellular or intracellular manner*. For the intracellular delivery and sustained release of nucleic acids, a lysosomalytic agent, e.g. an amphiphilic peptide, could be conjugated to the carriers to enhance the lysosomal escape after cell uptake. A lipophilic moiety, e.g. a group bearing cholesterol structural or lipid, could be conjugated to the carriers to enhance the interaction between coacervates and cell membrane therefore facilitate cell uptake. A nucleus localization signal could be conjugated to the carriers to facilitate the nucleus translocation.

Polyphosphate polymers of the invention are biodegradable, such polymers have a cleavable backbone, which is cleaved by at least one pathway selected from hydrolytic or enzymatic degradation.

Polyphosphate polymers of the invention are biocompatible before, during and after biodegradation. Biodegradation breakdown products are typically non-toxic. The polyphosphoramidate polymers of the invention are less cytotoxic poly-L-lysine, PEI and

liposome compositions *in vitro*. In one of the embodiment, polymer of Formula I degrades to phosphate, 1,2-propanediol and ethanolamine. The cytotoxicity assay suggests minimal toxicity when incubated with cells for 24 hours at a concentration higher than 500 µg/ml.

5

Polyphosphates suitable for use in the invention may be modified to comprise one or more specific ligands conjugated to the side chain or as a side chain group to enhance the cellular uptake of one or more bioactive molecules (nucleic acids and proteins) dispersed in carrier polymer and/or achieve tissue/cell specific delivery of the bioactive cargo.

10

Polyphosphates suitable for use in the methods of the present invention include any and all different single pure isomers and mixtures of two or more isomers. The term isomer is intended to include diastereoisomers, enantiomers, regioisomers, structural isomers, rotational isomers, tautomers, and the like. For compounds which contain one or more stereogenic centers, e.g., chiral compounds, the methods of the invention may be carried out with a enantiomerically enriched compound, a racemate, or a mixture of diastereomers. Preferred enantiomerically enriched compounds have an enantiomeric excess of 50% or more, more preferably the compound has an enantiomeric excess of 60%, 70%, 80%, 90%, 95%, 98%, or 99% or more.

15

20

Polyphosphates suitable for use in the methods of the present invention include any and all molecular weight distribution profiles, i.e., polymers having a  $M_w$ , or  $M_n$  of between 1 and about 50, more typically a  $M_w$ , or  $M_n$  between about 1.2 and about 10. Moreover, polyphosphoramidates of the invention have a polydispersity index of between about 1 and about 5.

25

As also discussed above, typical subjects for administration in accordance with the invention are mammals, such as primates, especially humans.

30

Biodegradable polymers differ from non-biodegradable polymers in that they can be degraded during *in vivo* therapy. This generally involves breaking down the polymer into its monomeric subunits. In principle, the ultimate hydrolytic breakdown products of polymers suitable for use in the methods of the present invention should be

5 biocompatible, non-toxic and easily excreted from a patient's body. However, the intermediate oligomeric products of the hydrolysis may have different properties. Thus, toxicology of a biodegradable polymer intended for implantation or injection, even one synthesized from apparently innocuous monomeric structures, is typically determined after one or more toxicity analyses.

10

The biodegradable polymer of the invention is preferably sufficiently pure to be biocompatible itself and remains biocompatible upon biodegradation. "Biocompatible" is defined to mean that the biodegradation products and/or the polymer itself are nontoxic and result in only minimal tissue irritation when instilled in the bladder or transported or  
15 otherwise localized to other tissues within a patient.

It will be appreciated that the actual preferred amounts of therapeutic agent or other component used in a given composition will vary according to the therapeutic agent being utilized including the polymer system being employed, the mode of application, the  
20 particular site of administration, etc. Optimal administration rates for a given protocol of administration can be readily ascertained by those skilled in the art using conventional dosage determination tests conducted with regard to the foregoing guidelines.

As used herein, "alkyl" is intended to include branched, straight-chain and cyclic  
25 saturated aliphatic hydrocarbon groups including alkylene, having the specified number of carbon atoms. Examples of alkyl include, but are not limited to, methyl, ethyl, n-propyl, i-propyl, n-butyl, s-butyl, t-butyl, n-pentyl, and s-pentyl. Alkyl groups typically have 1 to about 16 carbon atoms, more typically 1 to about 20 or 1 to about 12 carbon atoms. Preferred alkyl groups are C<sub>1</sub>-C<sub>20</sub> alkyl groups, more preferred are C<sub>1-12</sub>-alkyl and  
30 C<sub>1-6</sub>-alkyl groups. Especially preferred alkyl groups are methyl, ethyl, and propyl.

As used herein, "heteroalkyl" is intended to include branched, straight-chain and cyclic saturated aliphatic hydrocarbon groups including alkylene, having the specified number of carbon atoms and at least one heteroatom, e.g., N, O or S. Heteroalkyl groups will typically have between about 1 and about 20 carbon atoms and about 1 to about 8  
5 heteroatoms, preferably about 1 to about 12 carbon atoms and about 1 to about 4 heteroatoms. Preferred heteroalkyl groups include the following groups. Preferred alkylthio groups include those groups having one or more thioether linkages and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Alkylthio groups having 1, 2, 3, or 4 carbon  
10 atoms are particularly preferred. Preferred alkylsulfinyl groups include those groups having one or more sulfoxide (SO) groups and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Alkylsulfinyl groups having 1, 2, 3, or 4 carbon atoms are particularly preferred. Preferred alkylsulfonyl groups include those groups having one or more  
15 sulfonyl (SO<sub>2</sub>) groups and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Alkylsulfonyl groups having 1, 2, 3, or 4 carbon atoms are particularly preferred. Preferred aminoalkyl groups include those groups having one or more primary, secondary and/or tertiary amine groups, and from 1 to about 12 carbon atoms, more preferably from 1 to  
20 about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Aminoalkyl groups having 1, 2, 3, or 4 carbon atoms are particularly preferred.

As used herein, "heteroalkenyl" is intended to include branched, straight-chain and cyclic saturated aliphatic hydrocarbon groups including alkenylene, having the  
25 specified number of carbon atoms and at least one heteroatom, e.g., N, O or S. Heteroalkenyl groups will typically have between about 1 and about 20 carbon atoms and about 1 to about 8 heteroatoms, preferably about 1 to about 12 carbon atoms and about 1 to about 4 heteroatoms. Preferred heteroalkenyl groups include the following groups. Preferred alkylthio groups include those groups having one or more thioether linkages  
30 and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Alkenylthio groups having 1,

- 2, 3, or 4 carbon atoms are particularly preferred. Preferred alkenylsulfinyl groups include those groups having one or more sulfoxide (SO) groups and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Alkenylsulfinyl groups having 1, 2, 3, or 4 carbon atoms are particularly preferred.
- 5 Preferred alkenylsulfonyl groups include those groups having one or more sulfonyl (SO<sub>2</sub>) groups and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Alkenylsulfonyl groups having 1, 2, 3, or 4 carbon atoms are particularly preferred.
- 10 Preferred aminoalkenyl groups include those groups having one or more primary, secondary and/or tertiary amine groups, and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Aminoalkenyl groups having 1, 2, 3, or 4 carbon atoms are particularly preferred.
- 15 As used herein, "heteroalkynyl" is intended to include branched, straight-chain and cyclic saturated aliphatic hydrocarbon groups including alkynylene, having the specified number of carbon atoms and at least one heteroatom, e.g., N, O or S. Heteroalkynyl groups will typically have between about 1 and about 20 carbon atoms and about 1 to about 8 heteroatoms, preferably about 1 to about 12 carbon atoms and about 1 to about 4 heteroatoms. Preferred heteroalkynyl groups include the following groups.
- 20 Preferred alkynylthio groups include those groups having one or more thioether linkages and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Alkynylthio groups having 1, 2, 3, or 4 carbon atoms are particularly preferred. Preferred alkynylsulfinyl groups include
- 25 those groups having one or more sulfoxide (SO) groups and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Alkynylsulfinyl groups having 1, 2, 3, or 4 carbon atoms are particularly preferred. Preferred alkynylsulfonyl groups include those groups having one or more sulfonyl (SO<sub>2</sub>) groups and from 1 to about 12 carbon atoms, more preferably
- 30 from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Alkynylsulfonyl groups having 1, 2, 3, or 4 carbon atoms are particularly preferred.

Preferred aminoalkynyl groups include those groups having one or more primary, secondary and/or tertiary amine groups, and from 1 to about 12 carbon atoms, more preferably from 1 to about 8 carbon atoms, and still more preferably from 1 to about 6 carbon atoms. Aminoalkynyl groups having 1, 2, 3, or 4 carbon atoms are particularly preferred.

As used herein, "cycloalkyl" is intended to include saturated ring groups, having the specified number of carbon atoms, such as cyclopropyl, cyclobutyl, cyclopentyl, or cyclohexyl. Cycloalkyl groups typically will have 3 to about 8 ring members.

In the term "(C<sub>3-6</sub> cycloalkyl)C<sub>1-4</sub> alkyl", as defined above, the point of attachment is on the alkyl group. This term encompasses, but is not limited to, cyclopropylmethyl, cyclohexylmethyl, cyclohexylmethyl.

As used here, "alkenyl" is intended to include hydrocarbon chains of straight, cyclic or branched configuration, including alkenylene, and one or more unsaturated carbon-carbon bonds which may occur in any stable point along the chain, such as ethenyl and propenyl. Alkenyl groups typically will have 2 to about 12 carbon atoms, more typically 2 to about 12 carbon atoms.

As used herein, "alkynyl" is intended to include hydrocarbon chains of straight, cyclic or branched configuration, including alkynylene, and one or more triple carbon-carbon bonds which may occur in any stable point along the chain, such as ethynyl and propynyl. Alkynyl groups typically will have 2 to about 20 carbon atoms, more typically 2 to about 12 carbon atoms.

As used herein, "haloalkyl" is intended to include both branched and straight-chain saturated aliphatic hydrocarbon groups having the specified number of carbon atoms, substituted with 1 or more halogen (for example -C<sub>v</sub>F<sub>w</sub> where v = 1 to 3 and w = 1 to (2v+1)). Examples of haloalkyl include, but are not limited to, trifluoromethyl, trichloromethyl, pentafluoroethyl, and pentachloroethyl. Typical



haloalkyl groups will have 1 to about 16 carbon atoms, more typically 1 to about 12 carbon atoms.

As used herein, "alkoxy" represents an alkyl group as defined above with the indicated number of carbon atoms attached through an oxygen bridge. Examples of alkoxy include, but are not limited to, methoxy, ethoxy, n-propoxy, i-propoxy, n-butoxy, 2-butoxy, t-butoxy, n-pentoxy, 2-pentoxy, 3-pentoxy, isopentoxy, neopentoxy, n-hexoxy, 2-hexoxy, 3-hexoxy, and 3-methylpentoxy. Alkoxy groups typically have 1 to about 16 carbon atoms, more typically 1 to about 12 carbon atoms.

10

"Prodrugs" are intended to include any covalently bonded carriers which release the active parent drug according to formula I *in vivo* when such prodrug is administered to a mammalian subject. Prodrugs of a compound are prepared by modifying functional groups present in the drug compound in such a way that the modifications are cleaved, either in routine manipulation or *in vivo*, to the parent compound.

15

Combinations of substituents and/or variables are permissible only if such combinations result in stable compounds. A stable compound or stable structure is meant to imply a compound that is sufficiently robust to survive isolation to a useful degree of purity from a reaction mixture, and formulation into an effective therapeutic agent.

20

As used herein, the term "aliphatic" refers to a linear, branched, cyclic alkane, alkene, or alkyne. Preferred aliphatic groups in the poly(phosphoester-co-amide) polymer of the invention are linear or branched and have from 1 to 20 carbon atoms.

25

As used herein, the term "aryl" refers to an unsaturated cyclic carbon compound with  $4n+2$  electrons where  $n$  is a non-negative integer, about 5-18 aromatic ring atoms and about 1 to about 3 aromatic rings.

As used herein, the term "heterocyclic" refers to a saturated or unsaturated ring compound having one or more atoms other than carbon in the ring, for example, nitrogen, oxygen or sulfur.

5       The polymers of the invention are usually characterized by a release rate of the therapeutic agent in vivo that is controlled at least in part as a function of hydrolysis of the phosphoester bond of the polymer during biodegradation. Additionally, the therapeutic agent to be released may be conjugated to the sidechain of the phosphoramidate repeat unit to form a pendant drug delivery system. Further, other factors  
10       are also important.

The life of a biodegradable polymer in vivo also depends upon its molecular weight, crystallinity, biostability, and the degree of cross-linking. In general, the greater the molecular weight, the higher the degree of crystallinity, and the greater the  
15       biostability, the slower biodegradation will be.

The therapeutic agent of the invention can vary widely with the purpose for the composition. The agent(s) may be described as a single entity or a combination of entities. The delivery system is designed to be used with therapeutic agents having high  
20       water-solubility as well as with those having low water-solubility to produce a delivery system that has controlled release rates. The terms "therapeutic agent" and "biologically active substance" include without limitation, medicaments; vitamins; mineral supplements; substances used for the treatment, prevention, diagnosis, cure or mitigation of disease or illness; or substances which affect the structure or function of the body; or  
25       pro-drugs, which become biologically active or more active after they have been placed in a predetermined physiological environment.

Non-limiting examples of useful therapeutic agents and biologically active substances include the following expanded therapeutic categories: anabolic agents,  
30       antacids, anti-asthmatic agents, anti-cholesterolemic and anti-lipid agents, anti-coagulants, anti-convulsants, anti-diarrheals, anti-emetics, anti-infective agents, anti-

inflammatory agents, anti-manic agents, anti-nauseants, anti-neoplastic agents, anti-obesity agents, anti-pyretic and analgesic agents, anti-spasmodic agents, anti-thrombotic agents, anti-uricemic agents, anti-anginal agents, antihistamines, anti-tussives, appetite suppressants, biologicals, cerebral dilators, coronary dilators, decongestants, diuretics,  
5 diagnostic agents, erythropoietic agents, expectorants, gastrointestinal sedatives, hyperglycemic agents, hypnotics, hypoglycemic agents, ion exchange resins, laxatives, mineral supplements, mucolytic agents, neuromuscular drugs, peripheral vasodilators, psychotropics, sedatives, stimulants, thyroid and anti-thyroid agents, uterine relaxants, vitamins, antigenic materials, and prodrugs.

10

Specific examples of useful therapeutic agents and biologically active substances, i.e., bioactive molecules, from the above categories include: (a) anti-neoplastics such as androgen inhibitors, antimetabolites, cytotoxic agents, immunomodulators; (b) anti-tussives such as dextromethorphan, dextromethorphan hydrobromide, nescapine,  
15 carbetapentane citrate, and chlophedianol hydrochloride; (c) antihistamines such as chlorpheniramine maleate, phenindamine tartrate, pyrilamine maleate, doxylamine succinate, and phenyltoloxamine citrate; (d) decongestants such as phenylephrine hydrochloride, phenylpropanolamine hydrochloride, pseudoephedrine hydrochloride, and ephedrine; (e) various alkaloids such as codeine phosphate, codeine sulfate and morphine;  
20 (f) mineral supplements such as potassium chloride, zinc chloride, calcium carbonates, magnesium oxide, and other alkali metal and alkaline earth metal salts; (g) ion exchange resins such as cholestyramine; (h) anti-arrhythmics such as N-acetylprocainamide; (i) antipyretics and analgesics such as acetaminophen, aspirin and ibuprofen; (j) appetite suppressants such as phenyl-propanolamine hydrochloride or caffeine; (k) expectorants  
25 such as guaifenesin; (l) antacids such as aluminum hydroxide and magnesium hydroxide; (m) biologicals such as peptides, polypeptides, proteins and amino acids, hormones, interferons or cytokines and other bioactive peptidic compounds, such as hGH, tPA, calcitonin, ANF, EPO and insulin; (n) anti-infective agents such as anti-fungals, anti-virals, antiseptics and antibiotics; and (o) antigenic materials, particularly those useful in  
30 vaccine applications.

Preferably, the therapeutic agent or biologically active substance is selected from the group consisting of DNA, polysaccharides, growth factors, hormones, anti-angiogenesis factors, interferons or cytokines, and pro-drugs. In a particularly preferred embodiment, the therapeutic agent is a DNA vaccine comprising a DNA sequence  
5 encoding an antigen, a DNA sequence encoding a cytokine or a mixture of DNA sequences encoding an antigen and a cytokine.

Other preferred therapeutic agents are substances that are capable of modulating the immune response of a patient. Preferred therapeutic agents capable of modulating an  
10 immune response include protein vaccines or DNA vaccines. More preferred therapeutic agents capable of modulating an immune response are DNA vaccines. In general, DNA vaccine include vaccines which comprise a DNA sequence encoding an antigen, DNA sequence encoding a cytokine or a combination of DNA sequence encoding an antigen and DNA sequence encoding a cytokine.

15 Preferred cytokine additives suitable for use in a DNA vaccine include cytokines selected from interleukins or interferons which can shift a patient's immune response toward either a  $T_H1$  or  $T_H2$  response. Preferred cytokines suitable for use in modulating an immune response include interleukin-12, interleukin-10, interleukin-5, interleukin-4  
20 and interferon-gamma. Other preferred cytokines include interferon for use in treatment of Hepatitis C.

Suitable genes for use in the methods of the invention encode therapeutic proteins for administration locally such as for use in treatment of muscle related diseases, such as  
25 the neuromuscular disorders and also for systemic delivery of therapeutic proteins such as secretory therapeutic proteins including, for example, Interferon for use in treatment of Hepatitis C.

Methods of the present invention are suitable for any protein or DNA based  
30 vaccination method which induces either  $T_H1$   $T_H2$  or a combination of  $T_H1$  and  $T_H2$  immunological responses. Methods are applicable for any illness or disease for which a

vaccination is known or for which treatment is effected by systemic delivery of a therapeutic agent such as a small molecule drug, protein or DNA.

In preferred immune modulation methods of the invention, administration  
5 methods of the invention for delivering a therapeutic agent to the lymph nodes are suitable for delivering an therapeutic agent capable of modulating an immune response so that a patient's immune response is modulated. The lymph node is one of the primary sites for immune system stimulation; delivery of drugs, proteins, or DNA to these nodes results in the modulation of the immune response. After the microparticles are  
10 administered to the lymph nodes, they deliver their the therapeutic agent contained therein. Release of the therapeutic can be observed in by direct visualization of protein expression in cells of the lymph nodes, as well as indirect evidence through positive immune responses.

15 Other preferred therapeutic agents are substances that are capable of modulating the immune response of a patient. Preferred therapeutic agents capable of modulating an immune response include protein vaccines or DNA vaccines. More preferred therapeutic agents capable of modulating an immune response are DNA vaccines. In general, DNA vaccine include vaccines which comprise a DNA sequence encoding an antigen, DNA  
20 sequence encoding a cytokine or a combination of DNA sequence encoding an antigen and DNA sequence encoding a cytokine.

The therapeutic agents are used in amounts that are therapeutically effective. While the effective amount of a therapeutic agent will depend on the particular material  
25 being used, amounts of the therapeutic agent from about 1% to about 65% have been easily incorporated into the present delivery systems while achieving controlled release. Lesser amounts may be used to achieve efficacious levels of treatment for certain therapeutic agents.

30 In addition, the polymer composition of the invention can also comprise polymer blends of the polymer of the invention with other biocompatible polymers, so long as they

do not interfere undesirably with the biodegradable characteristics of the composition. Blends of the polymer of the invention with such other polymers may offer even greater flexibility in designing the precise release profile desired for targeted drug delivery or the precise rate of biodegradability desired for structural implants such as for orthopedic applications. Examples of such additional biocompatible polymers include other polycarbonates; polyesters; polyorthoesters; polyamides; polyurethanes; poly(iminocarbonates); and polyanhydrides.

As a drug delivery device, the polymer compositions of the invention provide a polymeric matrix capable of sequestering a biologically active substance and provide predictable, controlled delivery of the substance. The polymeric matrix then degrades to non-toxic residues.

It will be understood, however, that the specific dose level for any particular patient will depend upon a variety of factors including the activity of the specific compound employed, the age, body weight, general health, sex, diet, time of administration, route of administration, and rate of excretion, drug combination (i.e., other drugs being administered to the patient), the severity of the particular disease undergoing therapy, and other factors, including the judgment of the prescribing medical practitioner.

A positively chargeable biodegradable polymer composition of the invention also may be packaged together with instructions (i.e. written, such as a written sheet) for treatment of a disorder as disclosed herein, e.g. instruction for treatment of a subject that is susceptible to or suffering from a disease or disorder which may be treated by administration of a bioactive molecule, e.g., therapeutic agent, dispersed in the positively chargeable biodegradable polymer composition.

A positively chargeable biodegradable polymer composition of the invention be administered parenterally, preferably in a sterile non-toxic, pyrogen-free medium. The drug, depending on the vehicle and concentration used, can either be suspended or

dissolved in the vehicle. Advantageously, adjuvants such as local anesthetics, preservatives and buffering agents can be dissolved in the vehicle. The term parenteral as used herein includes injections and the like, such as subcutaneous, intradermal, intravascular (e.g., intravenous), intramuscular, intrasternal, spinal, intrathecal, and like  
5 injection or infusion techniques, with subcutaneous, intramuscular and intravascular injections or infusions being preferred.

A positively chargeable biodegradable polymer composition of the invention also may be packaged together with instructions (i.e. written, such as a written sheet) for  
10 treatment of a disorder as disclosed herein, e.g. instruction for treatment of a subject that is susceptible to or suffering from inflammation, cellular injury disorders, or immune system disorders.

The present invention provides biocompatible and biodegradable gene carriers  
15 that release the DNA to a targeted tissue, cell or fluid in a sustained manner. In one embodiment, the invention provides a PPE-EA polyphosphate as a gene carrier. The structure of PPE-EA is built on a phosphate backbone with a 1,2-propylene diol moiety, and a charged aminoethyl side chain. The ultimate hydrolytic degradation products of this polymer are expected to be  $\alpha$ -propylene glycol, phosphate and ethanolamine, all with  
20 minimal toxicity profiles. Such a design has led to a minimal toxicity profile of this polymer carrier, as demonstrated in the vigorous cytotoxicity assay, where gene carriers were incubated with cells for 24 hours. The acute tissue response to PPE-EA evaluated in mouse muscles also revealed a similar contrast, when compared with PEI at a same dose of positive charges.

25 PPE-EA has a relatively higher molecular weight compared with most other biodegradable gene carriers known in the art. The relatively high molecular weight of PPE-EA ( $\overline{M}_w$ : 30,300, degree of polymerization: 100.2) was achieved by ring opening polymerization of a cyclic phosphate monomer. This feature coupled with the pendent  
30 chain charges has increased the ability of PPE-EA to form condensate complexes with DNA. Complete binding of DNA was achieved with PPE-EA at a charge ratio of 1,

which was several folds lower than other biodegradable gene carriers. At this charge ratio, PPE-EA was shown to effectively protect plasmid DNA from DNase I degradation and serum degradation.

5           Applicants have also surprisingly discovered that the relatively high degradability of PPE-EA is suitable for the sustained release of DNA which occurs in connection with degradation of the polymeric phosphate carrier. DNA release occurred as early as a few hours at the low N/P ratios, to a few days of retardation for high N/P ratios. N/P ratio was the factor that dominated the kinetics of DNA release, especially in the first phase (within  
10 the first 6 days), during which period the DNA release rate decreased with the increase of N/P ratio. Such an adjustable DNA release kinetics is potentially advantageous in achieving different intracellular and extracellular sustained release of DNA. Nevertheless, the DNA release rate should be optimized for each particular application.

15           The PPE-EA/DNA complexes of the invention offer superior controlled release profiles when compared with the biodegradable polymer based systems described in the literature, e.g. PLGA and polyanhydride micro/nanoparticles. Loading levels of DNA achieved in this system were much higher than that in PLGA microparticles. For example, PPE-EA/DNA complexes with a N/P ratio of 1 have a DNA payload of 60%,  
20 comparing with less than 2% for PLGA or polyanhydride microspheres. Higher loading level reduced the use of carriers significantly. Moreover, the PPE-EA/DNA system was prepared by complex coacervation versus the double emulsion method for the microsphere systems. The former involved only aqueous conditions at room temperature, whereas the latter involved organic solvent and sonication/vortexing. The mild  
25 preparation conditions yielded good structural and functional integrity of the DNA released from PPE-EA/DNA complexes.

          The sustained gene delivery system provided by the present invention is suitable for use in administration of gene delivery intramuscularly. This has to be compared to  
30 naked DNA injection, which is somewhat effective in affording both local and systemic transgene expression. Intramuscular administration of PPE-EA/DNA complexes resulted



in significantly higher and delayed  $\beta$ -gal expression in muscle, although the enhancement effect becomes less prominent at higher administration dose. The higher  $\beta$ -gal level in the PPE-EA mediated gene transfer is presumably due to the sustained release of plasmid at the injection site and the protection of plasmid by PPE-EA. Compositions of a positively chargeable phosphate polymer and DNA provided by the present invention which have a lower N/P ratio ( $<1$ ) achieved higher levels of gene expression, suggesting the complicated mechanism in gene delivery to skeletal muscle. Compositions having higher N/P ratios such as 1.5 or 2 gave background level of gene expression in the muscle. This diminished gene expression was not likely due to any toxicity of PPE-EA in the complexes at higher N/P ratio, since the total amount of PPE-EA used in this formulation was only 20% of the dose tested for the tissue compatibility experiment. Muscle biopsy in these groups did not show any noticeable toxicity either. This is also consistent with the results from other cationic polymer/DNA complexes in muscle injection formulation, where no positive gene transfection has been reported. A recent study revealed that intramuscular injection of PEI/DNA complexes induces gene expression in central nervous system (e.g. brain stem) through retrograde transport of the complexes/particles (13). It is unclear yet if these PPE-EA/DNA complexes were transported out of the muscle in a similar manner.

This enhancement of gene expression may be applied to deliver therapeutic proteins to systemic circulation such as the delivery of IFN- $\alpha$ 2b. This is a secretory protein that has a serum half-life of 1.7 hours (14). An N/P ratio of 0.5 has been selected due to its higher efficiency in the previous study. Following intramuscular injection, PPE-EA/DNA complexes generated 1.8 times higher IFN- $\alpha$ 2b in blood circulation than naked DNA on day 14 ( $p < 0.05$ ), although at other time points, the expression levels were similar to that of naked DNA injection. This is particularly significant because of the short half-life of IFN- $\alpha$ 2b. It is worth noting that this result was obtained at a relatively higher dose of DNA (50  $\mu$ g). As suggested by the  $\beta$ -gal experiment, the enhancement effect by PPE-EA/DNA complexes might be more significant at lower doses.

The positively chargeable biodegradable polyphosphates provided by the present invention are the first polymeric carriers capable of inducing higher levels of gene expression in muscle than naked DNA. Although the experimental protocol was far from optimized, these results suggested the potential of PPE-EA as a gene carrier for the local delivery as well as systemic delivery of protein pharmaceuticals.

In one embodiment, the present invention provides a novel controlled gene delivery system based on a water soluble and biodegradable polyphosphoester, poly(2-aminoethyl propylene phosphate) [PPE-EA]. The polymer degraded in PBS at 37 °C through the cleavage of the backbone phosphate bonds, and it was synthesized with a relative high molecular weight to ensure a suitable hydrolytic stability as a gene carrier. The tissue response and cytotoxicity study demonstrated a better tissue compatibility of PPE-EA in mouse muscle compared to commonly used polyethylenimine and poly-L-lysine. PPE-EA condensed DNA efficiently and protected DNA from nuclease and serum degradation. Sustained release of plasmid was achieved from PPE-EA/DNA complexes as a result of PPE-EA degradation. The DNA release profiles appear to be predominantly controlled by carrier degradation and the release rate of plasmid could be adjusted by varying the charge ratio of PPE-EA to DNA. At an N/P (amino to phosphate groups) ratio of 1, a 46% burst was observed for the first day, followed by about 4% release per day (24 µg DNA/day/mg of complex) for 12 days. Higher charge ratios reduced both the DNA release rate and the burst effect. The released DNA retained its structural and functional integrity. Intramuscular injection of PPE-EA-p43-LacZ complexes at N/P ratios of 0.5 and 1 resulted in enhanced β-galactosidase expression in anterior Tibialis muscle in Balb/c mice, as compared with naked DNA injections. Similarly, PPE-EA/IFNα2b DNA complexes generated an increased systemic level of interferon-α2b in mouse serum following intramuscular injection, as compared with naked DNA injection.

The following examples are illustrative of the invention. All documents mentioned herein are incorporated herein by reference.

#### EXAMPLES:

The following examples are offered by way of illustration and are not intended to limit the invention in any manner.

**Example 1. Synthesis and characterization of polyphosphoramidates**

5     The synthetic scheme is shown in Figure 1.

1.1 Synthesis of poly(4-methyl-2-oxo-2-hydro-1,3,2-dioxaphospholane)

1.2

4-methyl-2-oxo-2-hydro-1,3,2-dioxaphospholane (58g, 0.475mol) [freshly prepared according to Lucas' method (*Lucas, Mitchell, and Scully, 1950, Cyclic phosphites of some aliphatic glycols. J. Am. Chem. Soc. 72: 5491-5497*) was polymerized in 200ml of fresh dried  $\text{CHCl}_3$  at room temperature for 48 hours. Polymerization was initiated with triisobutylaluminum (1wt%, 4 ml of 15% solution in heptane). The polymer was obtained by precipitation into anhydrous benzene. This polymer became insoluble in chloroform after precipitation, but it is soluble in anhydrous DMF.

15

1.2 Synthesis of poly(4-methyl-2-oxo-2-chloro-1,3,2-dioxaphospholane)

40mL of polymer solution from the former step was added into 200 ml of dried benzene. The precipitate was dried under vacuum and weighted to obtain white polymer (4.187g). This polymer was then suspended in dried  $\text{CH}_2\text{Cl}_2$  and dry  $\text{Cl}_2$  was passed. The suspension was dissolved during chlorination. Addition of  $\text{Cl}_2$  was stopped at the first appearance of a persistent yellow color. The excess of  $\text{Cl}_2$  was removed under vacuum until a colorless solution resulted. This solution was further used for preparation of different derivatives without polymer isolation.

20

25     1.3 Synthesis of Poly(4-methyl-2-oxo-2-(N-benzylloxycarbonyl)-aminoethoxy-1,3,2-dioxaphospholane)

To the cooled solution of poly(4-methyl-2-oxo-2-chloro-1,3,2-dioxaphospholane) (24.4 mmol of P-Cl) in  $\text{CH}_2\text{Cl}_2$  from the former step, was added DMAP (6.56 g, 53.6 mmol), then the solution of benzyl N-(2-hydroxyethyl) carbamate (5.24 g, 26.9 mmol) was added dropwise from an addition funnel. After the addition, the mixture was heated and the mixture was allowed to reflux for 48 hours. The solution was washed with 1N

30

HCl twice and water twice. The organic layer was dried over anhydrous magnesium sulfate and concentrated. The product was obtained by pouring the concentrated solution into ether as a white glassy solid (4.6 g, yield 60%).

5    1.4 Synthesis of poly(4-methyl-2-oxo-2-aminoethyloxy-1,3,2-dioxaphospholane)

Remove of the Cbz group was accomplished using formic acid and Pd/C according to a reported method (*Zhou and Kohn, 1990, Preparation of poly(L-serine ester): A structural analogue of conventional poly(L-serine), Macromolecules 23: 3399-3406*). In a 25 ml round-bottom flask the polymer (300 mg) was dissolved in 4 ml  
10 of DMF. To this solution under a N<sub>2</sub> atmosphere was added 1 g of Pd/C (10%, Aldrich). With vigorous stirring formic acid (14 ml) was added dropwise over 15 min. The reaction was stirred at room temperature for 14 hours and filtered to remove Pd/C. The catalyst was washed with 20 ml of 1N HCl. The filtrates were combined and concentrated under vacuum using a water bath below 45 °C to a volume of 5 ml whereupon 10 ml of 1N HCl  
15 was added. The solution was reconcentrated as above to a volume of 1 ml and then added dropwise to 150 ml of acetone with stirring and cooled to -20 °C. The polymer was isolated and dried thoroughly under vacuum. Yield 166 mg (80%). The structure of PPE-EA was confirmed by NMR. The weight average molecular weight of PPE was 38,800 with a polydispersity index of 1.64 as determined by GPC/LS/RI method (Figure 2).

20

**Example 2. Assay for the cytotoxicity of PPE-EA.**

Cytotoxicity of PPE-EA in comparison with other potential gene carriers [poly-L-lysine (PLL) and polyethylenimine (PEI)] is evaluated using the MTT assay. COS-7 cells (6,000 per well) were seeded in 96-well plates and incubated for 24 hours at 37 °C in 5%  
25 CO<sub>2</sub> followed by adding polymer solutions (50 µl) at different concentrations (0-1 mg/ml). After 24 hours incubation, cell viability was analyzed by a MTT assay according to Hansen's method (*Hansen, et al., 1989, J. Immunol. Methods, 119: 203-210*).

The assay results showed no significant change in morphology and proliferation  
30 rate as compared with cells without treatment, when PPE-EA was incubated with cells for 24 hours at a dose up to 0.5 mg/ml. In contrast, LD<sub>50</sub> values of PEI and PLL in this assay

were below 10 µg/ml (Figure 3). Similar results were observed in HEK 293 cells. This suggested that PPE-EA have a minimal cytotoxicity.

**Example 3. Gel retardation assay for the DNA binding capacity of PPE-EA.**

5        To 2 µg of plasmid DNA dissolved in 20 µl of saline was added a PPE-EA solution in 20 µl of saline at the increasing charge ratios from 0.5 to 10 respectively. The mixture was vortexed for 20 seconds and the coacervates were incubated at room temperature for 30 minutes and then 10 µl of coacervates was analyzed on a 0.8% agarose gel. Formation of coacervates between plasmid DNA and PPE-EA was confirmed by gel  
10    retardation assay (Figure 4). Complete binding of plasmid DNA was achieved at a charge ratio (N/P ratio) of 1 and above. PPE-DNA coacervates at charge ratio of 1 and above provided partial protection to plasmid DNA from nuclease degradation.

**Example 4. Preparation of coacervates and release of plasmid DNA from PPE-DNA  
15    coacervates**

      PPE-EA-DNA coacervates were prepared in PBS with 1mM EDTA by mixing plasmid DNA (60 µg/ml) with PPE-EA solution with concentration ranging from 20 µg/ml to 80 µg/ml to achieve various charge ratios (0.5 to 2). The coacervates were incubated at room temperature for 30 minutes before use. Plasmid DNA release from the  
20    coacervates was performed at 37°C. At various time points, samples were centrifuged and DNA concentration in the supernatant was measured by UV spectrophotometry at 260nm. The integrity of DNA released from the coacervates was analyzed by gel electrophoresis (0.8% agarose gel).

      Plasmid DNA released from PPE-EA-DNA coacervates over a period of two  
25    weeks when the coacervates were incubated in PBS. A sustained release profile for up to two weeks from the coacervates was observed as a result of degradation of PPE. The release rate was a function of charge ratio (Figure 5). When the coacervates were prepared at a N/P ratio of 1, a burst of 14.1 µg/ml was observed for the first day, then followed by a near constant release of 1.24 µg/ml/day for 12 days. At a N/P ratio of 1.5,  
30    DNA release followed first order release for the first week and then was near constant for the next week at a rate of 1.1 µg/ml/day. Whereas at a charge ratio of 2, DNA released at

a slower rate, with an average of 3.2  $\mu\text{g/ml/day}$  for the first 4 days and then 0.8  $\mu\text{g/ml/day}$  for the next nine days. No burst effect was observed for N/P ratios of 1.5 and above. DNA release from these PPE-EA-DNA coacervates remained intact as indicated by the gel electrophoretic analysis, although some nicking of plasmid occurred during the incubation.

#### Example 5. Transfection efficiency of PPE-EA-DNA complex in HEK293 cells

*In vitro* transfection of HEK293 cells with PPE-EA-DNA coacervates was evaluated using luciferase as a marker gene. Cells were seeded 24 hours prior to transfection into a 24-well plate (Becton-Dickinson, Lincoln Park, NJ) at a density of  $8 \times 10^4$  per well with 1 ml of complete medium (DMEM containing 10% FBS, supplemented with 2 mM L-glutamate, 50 units/ml penicillin and 50  $\mu\text{g/ml}$  streptomycin). At the time of transfection, the medium in each well was replaced with 1 ml of serum free DMEM. PPE-EA-DNA coacervates or PEI-DNA complexes or PLL-DNA complexes were incubated with the cells for 3 hours at 37 °C. The medium was replaced with 1 ml of fresh complete medium and cells were further incubated for 48 hours. All the transfection tests were performed in triplicate. After the incubation, cells were permeabilized with 200  $\mu\text{l}$  of cell lysis buffer (Promega Co., Madison, WI). The luciferase activity in cell extracts was measured using a luciferase assay kit (Promega Co., Madison, WI) on a luminometer (Lumat9605, EG&G Wallac). The light units (LU) were normalized against protein concentration in the cell extracts, which was measured using BCA protein assay kit (Pierce, Rockford, IL).

Figure 6 showed the transfection efficiency of PPE-EA-DNA coacervates prepared at different charge ratios. As the gel electrophoresis analysis showed, at a +/- charge ratio of 1.0 and above, all the plasmid DNA added to the preparation mixture complexed with PPE-EA. However, coacervates with a charge ratio lower than 4 failed to show significant gene expression level. The highest level of gene transfection was observed with the coacervates synthesized at +/- charge ratios between 6 and 8.

The transfection ability of PPE-EA-DNA coacervates suggested that the controlled release feature of this gene delivery technology could also be beneficial in an intracellular gene delivery application.

Chloroquine was shown to enhance the transfection efficiency of PPE-EA-DNA coacervates *in vitro*. Figure 6 also included the transfection efficiency of PPE-EA-DNA coacervates with 100 µg/ml of CQ as a comparison. It was evident that CQ can enhance the transfection efficiency for about 10 to 100 times at this concentration. The enhancement effect was more prominent for the coacervates prepared at lower charge ratio, suggesting the competition between the endosomal escape and DNA release and degradation inside the cells.

**Example 6. β-Galactosidase expression in mouse muscle following intramuscular injection**

Balb/c mice (three per group) received bilateral injections in the anterior tibialis muscle of 2 µg of p43-LacZ, or PPE-p43-LacZ coacervates prepared in saline at different charge ratios (0.5 and 1.0). The injected muscles were isolated on day 1, 3, 7 and 14. The expression level of β-galactosidase in the muscle was measured using a β-Gal Reporter Gene Assay kit (Roche Molecular Biochemicals) using β-galactosidase as a standard.

Intramuscular injection of PPE-p43-LacZ complexes at an N/P ratio of 0.5 resulted in a sustained level of β-galactosidase expression in anterior tibialis muscle in Balb/c mice. At a dose of 2 µg of DNA per muscle, PPE-DNA complexes with an N/P ratio of 0.5 yielded a 20-fold higher β-Gal expression on day 7 than naked DNA group and the gene expression level persisted for upto 4 weeks (Figure 7). Interestingly, complexes with an N/P ratio of 1, although had a delayed gene expression than naked DNA injection, yielded a lower level of β-Gal expression than complexes at N/P ratio of 0.5. A different set of experiment with a dose of 10 µg of DNA injection showed the similar trend.

**Example 7. Tissue response of PPE-EA in mouse muscle**

PPE-EA or PEI dissolved in saline (40 µl) was injected into the tibialis anterior muscle in Balb/c mice at a dose equivalent to 60 nmol of positive charge (13.1 µg/40 µl

for PPE-EA and 2.5 µg/40 µl for PEI). The muscles received the polymer injections were isolated at days 7, fixed in phosphate buffered formalin (10%), washed, and embedded in paraffin. Tissue sections were cut with 8 µm in thickness, placed on gelatin coated slides, and stained with hematoxylin and eosin (H&E) for histological examination. The tissue response was evaluated by an independent pathologist. Mice receiving intramuscular injection of 40 µl of saline were used as a control for this experiment.

Six to eight-week-old female Balb/c mice were obtained and housed in National University of Singapore Animal Holding Unit. Mice were maintained on ad libitum rodent feed and water at room temperature, 40% humidity. All animal procedures were approved by the National University of Singapore Faculty of Medicine Animal Care and Use Committee.

The acute tissue response to PPE-EA was evaluated in muscles in Balb/c mice, using saline and PEI injections as controls. PPE-EA and PEI were given at the same dose of positive charge (60 nmol of amino groups for PPE-EA and 60 nmol of total amino groups for PEI), to allow for a fair comparison with the assumption that the toxicity of these polymers predominantly stems from their cationicity. As a result, PPE-EA was given at a higher amount, 5.2 folds higher than PEI in mass (13.1 µg of PPE-EA versus 2.5 µg of PEI per injection). Histological analysis at day 7 revealed mild inflammatory reaction at muscle sites injected with the PPE-EA (Figure 8), whereas severe inflammatory response was observed in the PEI group. Moreover, severe necrosis was noticeable in all the muscle samples receiving PEI injection, with a large amount of macrophages, histiocytes and neutrophils present at the injection sites.

**Example 8. Delivery of interferon-α2b to systemic circulation using PPE-EA/DNA complexes**



A plasmid, pCMV-IVS-IFN-mod2, encoding interferon- $\alpha$ 2b (IFN- $\alpha$ 2b) was used to test the effectiveness of PPE-EA as a carrier for the systemic delivery of secretory proteins via intramuscular injection. It was provided by The Immune Response Corporation (Carlsbad, CA) as a gift.

- 5 pCMV-IVS-IFN-mod2 plasmid DNA was dissolved in saline at a concentration of 1.25 mg/ml. Complexes were prepared by adding 40  $\mu$ l of PPE-EA solution (0.41 mg/ml in saline) to 40  $\mu$ l of DNA solution containing 50  $\mu$ g DNA to achieve the N/P ratio of 0.5 and vortexed for about 20 seconds. The complexes were incubated at room temperature for 60 minutes. Balb/c mice (6 to 8 weeks old, five to seven mice per group) received
- 10 bilateral injections in the tibialis anterior muscle of 40  $\mu$ l of complexes containing 25  $\mu$ g of DNA. One group of mice received bilateral injections of 25  $\mu$ g of plasmid DNA in 40  $\mu$ l of saline, and another group of mice receiving 40  $\mu$ l of saline was used as the background control. The mice were bled at days 6, 10, 14 and 21, and serum samples were isolated and stored at -80 °C until assay. The concentrations of interferon- $\alpha$ 2b in
- 15 serum at different time points were analyzed using a human IFN- $\alpha$  ELISA kit (Pierce Endogen, Inc. Woburn, MA).

- No significant level of IFN- $\alpha$ 2b was detected in mice received 50  $\mu$ g of naked DNA injection until day 14, reaching 917 pg/ml and 790 pg/ml of IFN- $\alpha$ 2b in serum on day 14 and 21, respectively. Comparing with naked DNA injection, PPE-EA mediated
- 20 gene transfer yielded a higher serum IFN- $\alpha$ 2b of 1.61 ng/ml on day 14 ( $p < 0.05$ ), although IFN- $\alpha$ 2b concentration in serum declined to similar level as naked DNA on day 21 (Figure 9).

What is claimed is:

1. A positively chargeable biodegradable polymer comprising at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage.

2. A positively chargeable biodegradable polymer of claim 1 that is capable of forming a complex with negatively charged or neutral biologically active substances.

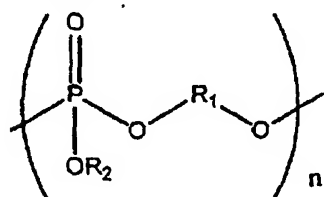
3. A positively chargeable biodegradable polymer of claim 2, wherein the negatively charged or neutral biologically active substances are selected from the group consisting of DNA, RNA, proteins, and small molecule therapeutics.

4. A positively chargeable biodegradable polymer of claim 2 or 3, wherein the biodegradable polymer is capable of complexing 20-60% by weight of the negatively charged or neutral biologically active substance.

5. A positively chargeable biodegradable polymer of claim 1, wherein the biodegradable polymer has between about 5 and about 2,000 phosphate groups in the backbone.

6. A positively chargeable biodegradable polymer of claim 1, wherein the biodegradable polymer has a molecular weight of between about 1000 and 1,000,000.

7. A positively chargeable biodegradable polymer of claim 1, according to Formula I:



FORMULA I

wherein

$R_1$  is a divalent organic moiety that is aliphatic, aromatic or heterocyclic;

$R_2$  is alkyl, aryl, heteroaryl, heteroalicyclic, cycloalkyl, aralkyl or cycloalkylalkyl;

and

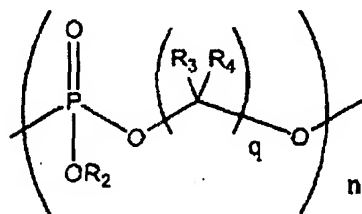
- 5 each occurrence of  $R_2$  is substituted with one or more positively chargeable functional groups.

8. A positively chargeable biodegradable polymer of claim 7, wherein  $R_2$  is substituted with one or more charged groups selected from the group consisting of  
10 primary amine, secondary amine, tertiary amine, quaternary amine.

9. A positively chargeable biodegradable polymer of claim 7, wherein  $R_1$  or  $R_2$  is substituted with one or more groups capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance.  
15

10. A positively chargeable biodegradable polymer of claim 9, wherein the group capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance is a lysosomalytic agent, an amphiphilic peptide, a steroid derivative.  
20

11. A positively chargeable biodegradable polymer of claim 7 according to formula II:



FORMULA II

- 25 wherein

$R_2$  is as defined in claim 7;

$R_3$  and  $R_4$  are independently selected at each occurrence of  $R_3$  and  $R_4$  from the group consisting of hydrogen, alkyl, cycloalkyl, alkoxy, aryl, heteroaryl, heteroalicyclic; aralkyl, a steroid derivative; and

$q$  is an integer from about 1 to about 5.

5

12. A positively chargeable biodegradable polymer composition comprising:

(a) at least one biologically active substance; and

(b) A positively chargeable biodegradable polymer comprising at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage.

10

13. A positively chargeable biodegradable polymer composition of claim 9, wherein the biologically active substance(s) are negatively charged or neutral biologically active substances.

15

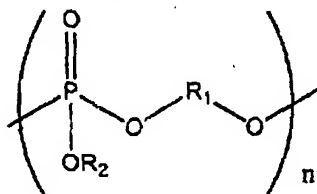
14. A positively chargeable biodegradable polymer composition of claim 13, wherein the negatively charged or neutral biologically active substances are selected from the group consisting of DNA, RNA, proteins, and small molecule therapeutics.

20

15. A positively chargeable biodegradable polymer composition of any one of claims 12-14, wherein the biodegradable polymer is capable of complexing 20-60% by weight of the negatively charged or neutral biologically active substance.

25

16. A positively chargeable biodegradable polymer composition of claim 12, wherein the positively chargeable biodegradable polymer is a polymer according to Formula I:



## FORMULA I

wherein

$R_1$  is a divalent organic moiety that is aliphatic, aromatic or heterocyclic;

$R_2$  is alkyl, aryl, heteroaryl, heteroalicyclic, cycloalkyl, aralkyl or cycloalkylalkyl;

5 and

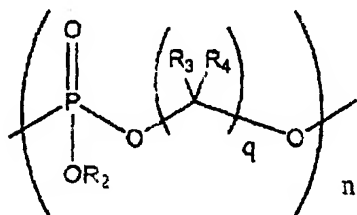
each occurrence of  $R_2$  is substituted with one or more positively chargeable functional groups.

17. A positively chargeable biodegradable polymer composition of claim 16,  
10 wherein  $R_2$  is substituted with one or more charged groups selected from the group consisting of primary amine, secondary amine, tertiary amine, quaternary amine.

18. A positively chargeable biodegradable polymer composition of claim 16,  
15 wherein  $R_1$  or  $R_2$  is substituted with one or more groups capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance.

19. A positively chargeable biodegradable polymer composition of claim 18,  
20 wherein the group capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance is a lysosomalytic agent, an amphiphilic peptide, a steroid derivative.

20. A positively chargeable biodegradable polymer composition of claim 16 according to formula II:



25 FORMULA II

wherein

$R_2$  is as defined in claim 16;

$R_3$  and  $R_4$  are independently selected at each occurrence of  $R_3$  and  $R_4$  from the group consisting of hydrogen, alkyl, cycloalkyl, alkoxy, aryl, heteroaryl, heteroalicyclic, aralkyl, a steroid derivative, and a cholesterol derivative; and

$q$  is an integer from about 1 to about 5.

5

21. A method of preparing a positively chargeable biodegradable polymer comprising the steps of:

polymerizing at least one monomer to form a polymer with at least one phosphoester linkage in the polymer backbone;

10 reacting the polymer with an alcohol having a positively chargeable group or a substituent that can be functionalized to a positively chargeable group under conditions conducive to the formation of a positively chargeable biodegradable polymer comprising at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain  
15 attached to the polymer backbone through a phosphoester linkage.

22. A method of preparing a positively chargeable biodegradable polymer of claim 21 wherein the positively chargeable biodegradable polymer is capable of forming a complex with one or more biologically active substances.

20

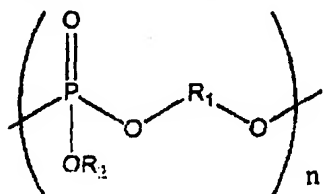
23. A method of preparing a positively chargeable biodegradable polymer of claim 21, wherein the biologically active substance(s) are selected from the group consisting of DNA, RNA, proteins, and small molecule therapeutics.

24. A method of preparing a positively chargeable biodegradable polymer of  
25 claim 22, wherein the biodegradable polymer is capable of complexing 20-60% by weight of the negatively charged or neutral biologically active substance.

25. A method of preparing a positively chargeable biodegradable polymer of claim 21, wherein the biodegradable polymer has between about 5 and about 2,000  
30 phosphate groups.

26. A method of preparing a positively chargeable biodegradable polymer of claim 21, wherein the biodegradable polymer has a molecular weight of between about 1000 and 1,000,000.

5 27. A method of preparing a positively chargeable biodegradable polymer of claim 21, according to Formula I:



FORMULA I

wherein

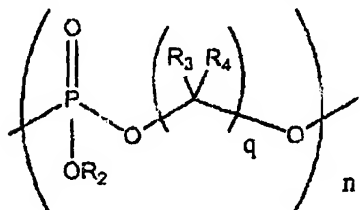
10  $R_1$  is a divalent organic moiety that is aliphatic, aromatic or heterocyclic;  
 $R_2$  is alkyl, aryl, heteroaryl, heteroalicyclic, cycloalkyl, aralkyl or cycloalkylalkyl;  
 and  
 each occurrence of  $R_2$  is substituted with one or more positively chargeable functional groups.

15 28. A method of preparing a positively chargeable biodegradable polymer of claim 27, wherein  $R_2$  is substituted with one or more charged groups selected from the group consisting of primary amine, secondary amine, tertiary amine, quaternary amine.

20 29. A method of preparing a positively chargeable biodegradable polymer of claim 27, wherein  $R_1$  or  $R_2$  is substituted with one or more groups capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance.

25 30. A method of preparing a positively chargeable biodegradable polymer of claim 29, wherein the group capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance is a lysosomalytic agent, an amphiphilic peptide, a steroid derivative.

31. A method of preparing a positively chargeable biodegradable polymer of claim 27 according to formula II:



FORMULA II

5 wherein

R<sub>2</sub> is as defined in claim 27;

R<sub>3</sub> and R<sub>4</sub> are independently selected at each occurrence of R<sub>3</sub> and R<sub>4</sub> from the group consisting of hydrogen, alkyl, cycloalkyl, alkoxy, aryl, heteroaryl, heteroalicyclic, aralkyl, a steroid derivative, and a cholesterol derivative; and

10 q is an integer from about 1 to about 5.

32. A method of preparing a positively chargeable biodegradable polymer composition comprising the steps of:

15 providing a positively chargeable biodegradable polymer comprising at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage.

20 contacting the positively chargeable biodegradable polymer with a biologically active substance under conditions conducive to the formation of a complex comprising the positively chargeable biodegradable polymer and the biologically active substance.

33. A method of preparing a positively chargeable biodegradable polymer composition of claim 32, wherein the negatively charged or neutral biologically active substances are selected from the group consisting of DNA, RNA, proteins, and small molecule therapeutics.

25



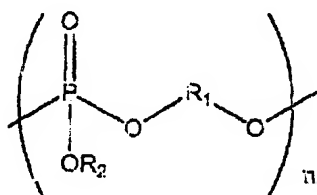
34. A method of preparing a positively chargeable biodegradable polymer composition of claim 32 or 33, wherein the biodegradable polymer is capable of complexing 20-60% by weight of the negatively charged or neutral biologically active substance.

5

35. A method of preparing a positively chargeable biodegradable polymer composition of claim 32, wherein the biodegradable polymer has between about 5 and about 2,000 phosphate groups.

10 36. A method of preparing a positively chargeable biodegradable polymer composition of claim 32, wherein the biodegradable polymer has a molecular weight of between about 1000 and 1,000,000.

15 37. A method of preparing a positively chargeable biodegradable polymer composition of claim 32, according to Formula I:



FORMULA I

wherein

$R_1$  is a divalent organic moiety that is aliphatic, aromatic or heterocyclic;

20  $R_2$  is alkyl, aryl, heteroaryl, heteroalicyclic, cycloalkyl, aralkyl or cycloalkylalkyl;  
and

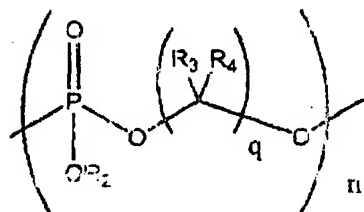
each occurrence of  $R_2$  is substituted with one or more positively chargeable functional groups.

25 38. A method of preparing a positively chargeable biodegradable polymer composition of claim 37, wherein  $R_2$  is substituted with one or more charged groups selected from the group consisting of primary amine, secondary amine, tertiary amine, quaternary amine.

39. A method of preparing a positively chargeable biodegradable polymer composition of claim 37, wherein  $R_1$  or  $R_2$  is substituted with one or more groups capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance.

40. A method of preparing a positively chargeable biodegradable polymer composition of claim 39, wherein the group capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance is a lysosomalytic agent, an amphiphilic peptide, a steroid derivative.

41. A method of preparing a positively chargeable biodegradable polymer composition of claim 37 according to formula II:



15 FORMULA II

wherein

$R_2$  is as defined in claim 37;

$R_3$  and  $R_4$  are independently selected at each occurrence of  $R_3$  and  $R_4$  from the group consisting of hydrogen, alkyl, cycloalkyl, alkoxy, aryl, heteroaryl, heteroalicyclic, aralkyl, a steroid derivative, and a cholesterol derivative; and

$q$  is an integer from about 1 to about 5.

42. A method for the controlled release of a biologically active substance comprising the steps of:

25 providing a positively chargeable biodegradable polymer composition comprising:

(a) at least one biologically active substance; and

(b) A positively chargeable biodegradable polymer comprising at least one phosphoester linkage in the polymer backbone and at least one positively chargeable group wherein the positively chargeable group is a substituent of a side chain attached to the polymer backbone through a phosphoester linkage;

5       contacting the composition in vivo or in vitro with a biological fluid, cell or tissue under conditions conducive to the delivery of at least a portion of the biologically active substance to the biological fluid, cell or tissue so that the biologically active substance is released in a controlled manner.

10       43. A method of claim 42, wherein the biologically active substance is released in-vivo.

44. A method of claim 42, wherein the biologically active substance is released in-vitro.

15       45. A method of claim 42, wherein the biologically active substance is released extracellularly.

20       46. A method of claim 42, wherein the biologically active substance is released intracellularly.

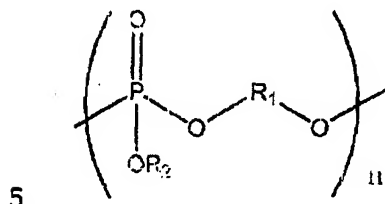
47. A method of claim 42, wherein the biologically active substance(s) are selected from the group consisting of DNA, RNA, proteins, and small molecule therapeutics.

25       48. A method of claim 47, wherein the biodegradable polymer is capable of complexing 20-60% by weight of the biologically active substance.

30       49. A method of claim 42, wherein the biodegradable polymer has between about 5 and about 2,000 phosphate groups.

50. A method of claim 42, wherein the biodegradable polymer has a molecular weight of between about 1,000 and 1,000,000

51. A method of claim 42, according to Formula I:



FORMULA I

wherein

R<sub>1</sub> is a divalent organic moiety that is aliphatic, aromatic or heterocyclic;

R<sub>2</sub> is alkyl, aryl, heteroaryl, heteroalicyclic, cycloalkyl, aralkyl or cycloalkylalkyl;

10 and

each occurrence of R<sub>2</sub> is substituted with one or more positively chargeable functional groups.

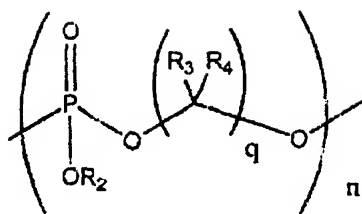
52. A method of claim 51, wherein R<sub>2</sub> is substituted with one or more charged groups selected from the group consisting of primary amine, secondary amine, tertiary amine, quaternary amine.

53. A method of claim 51, wherein R<sub>1</sub> or R<sub>2</sub> is substituted with one or more groups capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance.

54. A method of claim 53, wherein the group capable of facilitating intracellular delivery of a negatively charged or neutral biologically active substance is a lysosomalytic agent, an amphiphilic peptide, a steroid derivative.

25

55. A method of claim 51 according to formula II:



**FORMULA II**

wherein

$R_2$  is as defined in claim 47;

- 5  $R_3$  and  $R_4$  are independently selected at each occurrence of  $R_3$  and  $R_4$  from the group consisting of hydrogen, alkyl, cycloalkyl, alkoxy, aryl, heteroaryl, heteroalicyclic, aralkyl, a steroid derivative; and

$q$  is an integer from about 1 to about 5.

- 10 56. A method of claim 42, wherein the biologically active substance(s) are growth factor(s).

- 15 57. A method of claim 42, wherein the biologically active substance(s) is selected from the group consisting of DNA sequences, genes, gene fragments, DNA encoding vaccines, therapeutic agents, cytokines, immunoadjuvants, cancer therapeutic agents, proteins, and combinations thereof

58. A method of claim 57, wherein the biologically active substance(s) is a DNA sequence, a gene or a gene fragment.

20

- 59 A method of claim 58, wherein the DNA sequence, gene or gene fragment is administered in connection with gene therapy.

- 25 60. A method of claim 42 wherein the biologically active substance(s) modulates the immune response of the administered patient.

61. A method of claim 60, wherein the biologically active substance(s) is a protein vaccine or a DNA vaccine.

62. A method of claim 61, wherein the biologically active substance(s) is a  
5 DNA vaccine.

63. A method of claim 62, wherein the DNA vaccine comprises DNA encoding an antigen, DNA encoding a cytokine or a combination of DNA encoding an antigen and DNA encoding a cytokine.  
10

64. A method of claim 63, wherein the cytokine is selected from Interleukin or interferon which can shift a patient's immune response toward either a  $T_H1$  or  $T_H2$  response.

65. A method of claim 64, wherein the cytokine is selected from interleukin-12, interleukin-10, interleukin-5, interleukin-4, interferon-alpha or interferon-gamma.  
15

66. A method of any one of claims 42 through 65 wherein the positively chargeable biodegradable polymer composition is delivered in vivo.  
20

67. A method of claim 66 wherein the positively chargeable biodegradable polymer composition is delivered to a patient.

68. A method of claim 67 wherein the patient is a mammal.  
25

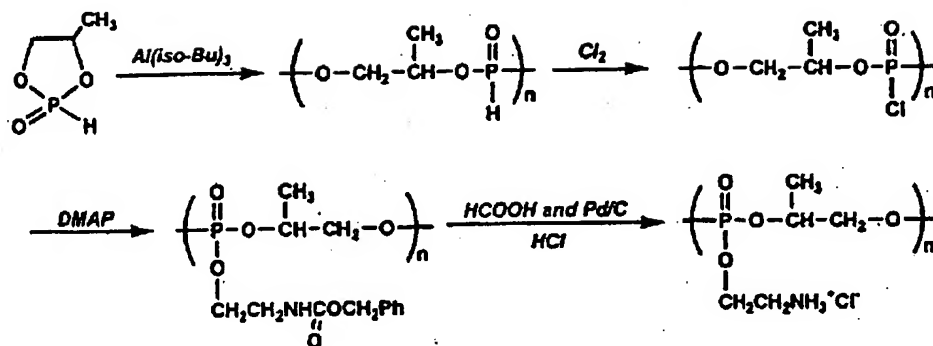
69. A method of claim 67 wherein the patient is a primate or human.

70. A method of any one of claims 67 through 69 in which the positively chargeable biodegradable polymer composition is delivered intramuscularly.  
30

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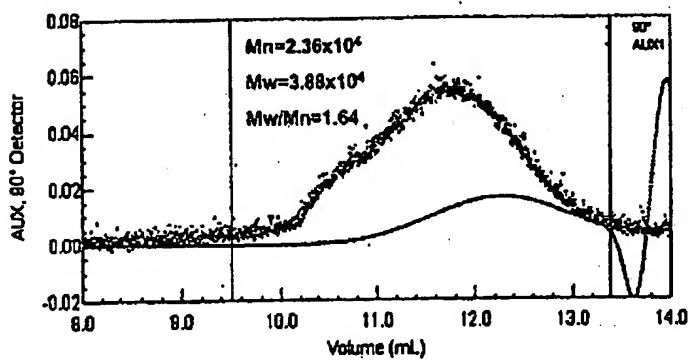
## FIGURES:

Figure 1.



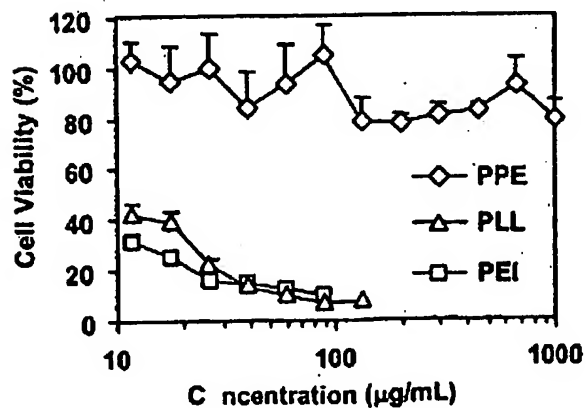
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Figure 2.



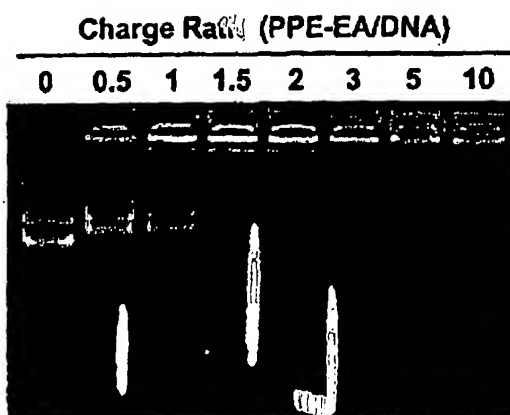
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Figure 3.



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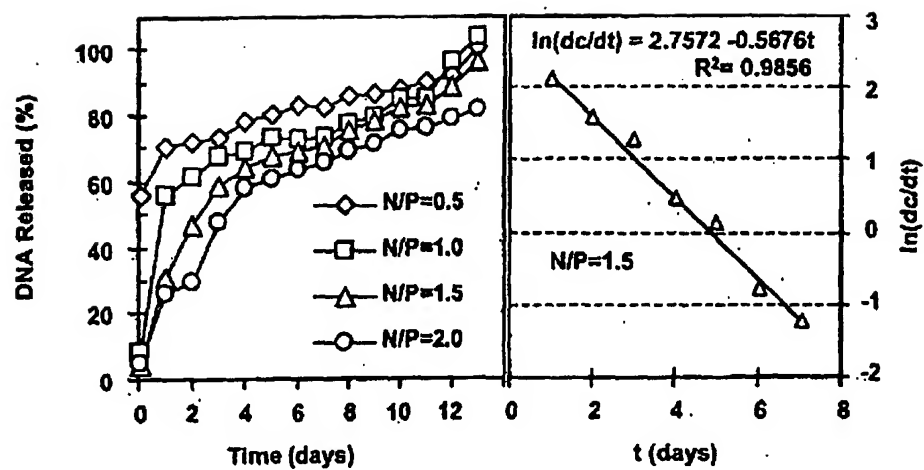
Figure 4.



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Figure 5.

10

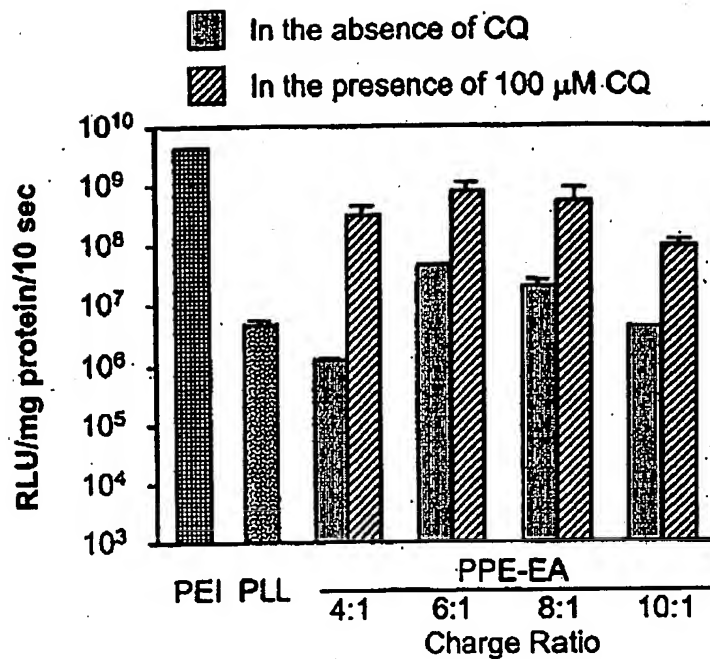


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-3/4-

Figure 6.



5

Figure 7.

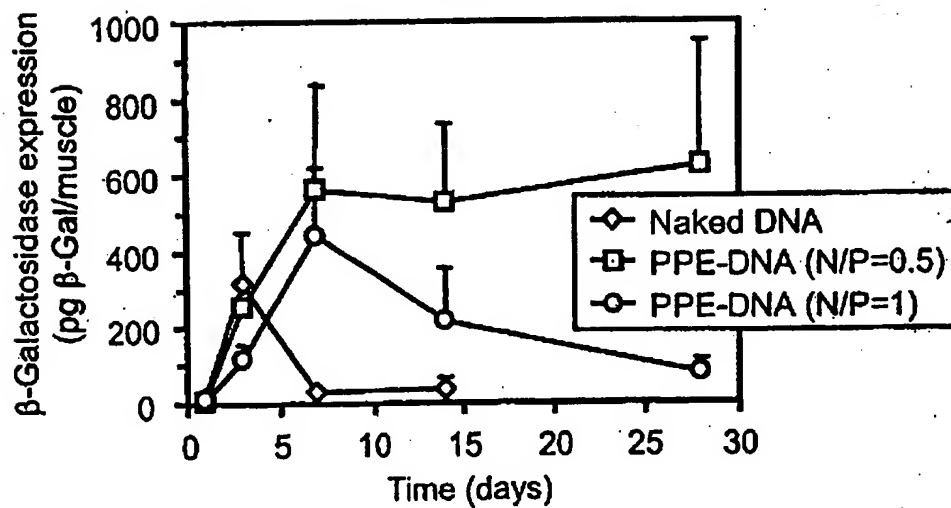
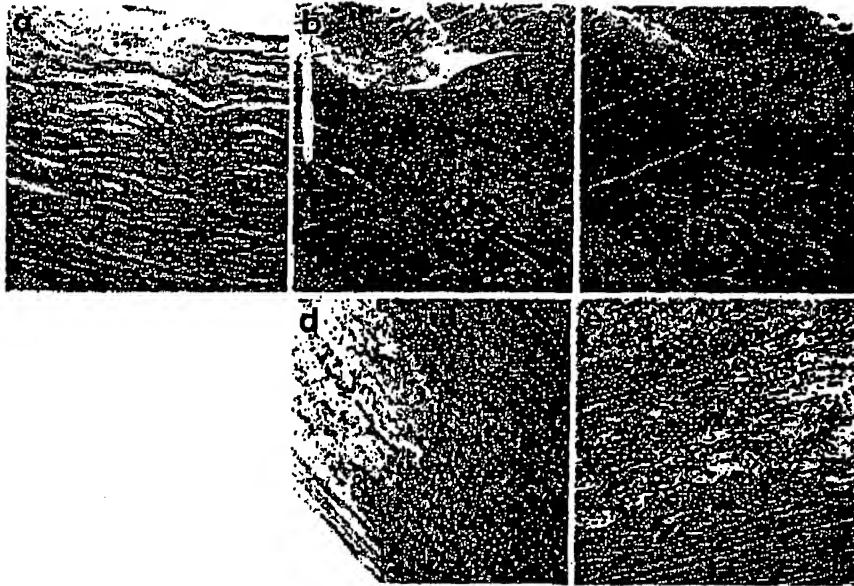
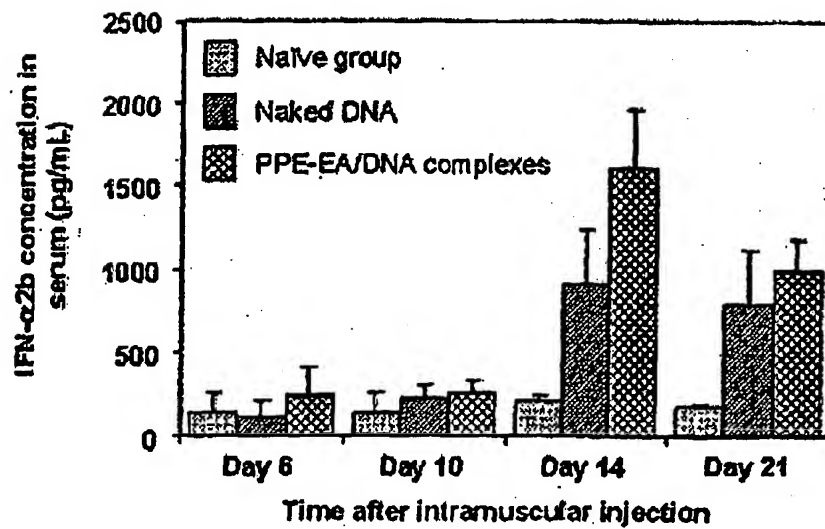


Figure 8



5

Figure 9



## INTERNATIONAL SEARCH REPORT

International application No.

PCT/SG02/00090

<b>A. CLASSIFICATION OF SUBJECT MATTER</b>		
Int. Cl. <sup>7</sup> : C08G 79/04, A61K 47/48, A61P 21/06, 11/06, 9/10, 1/08, 35/00, 11/02, 1/12, 1/10		
According to International Patent Classification (IPC) or to both national classification and IPC		
<b>B. FIELDS SEARCHED</b>		
Minimum documentation searched (classification system followed by classification symbols)		
IPC: C08G 79/04, A61K 47/48		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)		
WPAT & JAPIO (Search terms: phosphoester, biodegradable)		
<b>C. DOCUMENTS CONSIDERED TO BE RELEVANT</b>		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 194 581 A (LEONG) 16 March 1993 See column 4 line 19 to column 5 line 25, column 6 lines 29-68 and column 7 lines 36-55	1-70
X	US 5 952 451 A (ZHAO) 14 September 1999 See column 4 line 55 to column 6 line 30 and column 16 lines 40-54	1-70
X	US 6 166 173 A (MAO et al.) 26 December 2000 See claims 1, 5, 75 and 78	1-70
<input checked="" type="checkbox"/> Further documents are listed in the continuation of Box C <input checked="" type="checkbox"/> See patent family annex		
* "A"	Special categories of cited documents: document defining the general state of the art which is not considered to be of particular relevance	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"E"	earlier application or patent but published on or after the international filing date	"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"L"	document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"O"	document referring to an oral disclosure, use, exhibition or other means	"&" document member of the same patent family
"P"	document published prior to the international filing date but later than the priority date claimed	
Date of the actual completion of the international search 14 June 2002		Date of mailing of the international search report 24 JUN 2002
Name and mailing address of the ISA/AU AUSTRALIAN PATENT OFFICE PO BOX 200, WODEN ACT 2606, AUSTRALIA E-mail address: pct@ipaaustralia.gov.au Facsimile No. (02) 6285 3929		Authorized officer  ALBERT S. J. YONG Telephone No: (02) 6283 2160

## INTERNATIONAL SEARCH REPORT

International application No.

PCT/SG02/00090

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
P,X	US 6 322 797 B (MAO et al.) 27 November 2001 See column 3 line 53 to column 4 line 18	1-70
X	WO 98/46286 A (JOHNS HOPKINS UNIVERSITY SCHOOL OF MEDICINE) 22 October 1998 See claims 1, 30 and 63	1-70
X	WO 98/48859 A (GUILFORD PHARMACEUTICALS INC.) 5 November 1998 See claim 1	1-70
X	WO 99/00446 A (GUILFORD PHARMACEUTICALS INC.) 7 January 1999 See page 8 line 17 to page 10 line 4, claims 1 and 20	1-11, 21-31
X	WO 00/57852 A (GUILFORD PHARMACEUTICALS INC.) 5 October 2000 See page 18 line 21 to page 19 line 32, claims 1 and 17	1-70
P,X	WO 01/68052 A (JOHNS HOPKINS UNIVERSITY) 20 September 2001 See page 57 line 23 to page 58 line 11, claim 4	1-70

# INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No.

PCT/SG02/00090

This Annex lists the known "A" publication level patent family members relating to the patent documents cited in the above-mentioned international search report. The Australian Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent Document Cited in Search Report		Patent Family Member			
US	5194581	CA	2011171	EP	386757
		US	5256765	JP	3128938
US	5952451	AU	82611/98	EP	990008
		WO	9900446	US	6028163
US	6166173	AU	69449/98	BR	9809390
		HU	200001412	NO	994803
		WO	9844020	US	6376644
US	6322797	AU	69450/98	BR	9809064
		NO	994802	NZ	500649
				EP	973818
WO	9846286	AU	71206/98	US	5912225
				US	6238687
WO	9848859	AU	71771/98	BR	9809017
		HU	200001299	NO	995301
				EP	980269
WO	9900446	AU	82611/98	NO	336596
		US	5952451	US	6028163
WO	200057852	AU	200037625	BR	200009213
		EP	1185249	CZ	20013260
				NO	20014662
WO	200168052	AU	200147346		
END OF ANNEX					